Bone-free 3D Computed Tomography Angiography Using an Image-processing Application – Imaging Efficacy for Aneurysms Near the Skull Base and Clipped Cerebral Aneurysms

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Abstract
Bone-free 3D computed tomography angiography (CTA) can be carried out to image cerebral aneurysms near the skull base when the elimination of bones is surgically required. The maximum intensity projection (MIP) images were initially obtained using the application. Further post-processing was performed to obtain the MIP and volume-rendering (VR) images. This technique did not increase radiation exposure to patients, and remnant bones in the initial MIP images automatically acquired by the application for bone elimination could be easily removed through post-processing. Although parts of vessels were sometimes removed from the image along with the bones, these could be quickly and easily recovered through post-processing. Thus, bone-free 3D CTA and conventional 3D CTA are complementary tools for imaging cerebral aneurysms near the skull base prior to surgery. This application could also eliminate clips in cases of clipped cerebral aneurysms, and it could improve the accuracy of detecting remnant necks after clipping surgery.

Keywords
Computed tomography angiography (CTA), cerebral aneurysm, skull base, bone-free CTA, clipping surgery

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3D computed tomography angiography (3D CTA) is used to image cerebral aneurysms, steno-occlusive lesion of cerebral vessels and brain tumours. 3D CTA has become the accepted alternative to conventional intra-arterial digital subtraction angiography (IADSA) for imaging and detection of aneurysms1–5 and planning treatment. Multidetector (MD) CT allows a more precise evaluation of aneurysms with a shorter scanning time6 and better spatial resolution. Bony structures often disturb 3D CTA images near the skull base, and thus as a vessel-extraction technique, on the basis of the CT image registration, the subtraction of CT images of bony structures from CTA images has been developed;7–10 however, there are some limitations to this technique. For instance, subtle misregistration between the two CT images causes bone fractions in the subtracted images. More importantly, the two CT scans required for the technique expose the patient to two doses of radiation.

In an effort to address these concerns, a new image-processing application to eliminate bony structures and clipped cerebral aneurysms has been developed. This application has already been used for 3D CTA in patients with cerebral aneurysms near the skull base, and the efficacy of 3D CTA using this application for bone elimination has been evaluated.8 We also evaluated the efficacy of this technique in eliminating clip images in patients with clipped cerebral aneurysms.

Aneurysms
The cerebral aneurysms evaluated before surgery were determined to be located at the junction of the internal carotid artery (ICA) and the posterior communicating artery (PC). For the paracanaldoparacanoidal part of the ICA (paracanoidal aneurysm), at the junction of the ICA and the anterior choroid artery (Acho aneurysm), at the cavernous segment of the ICA (cavernous aneurysm), at the junction of the ICA and the ophthalmic artery (IC-oph aneurysm), at the terminal portion of the ICA (IC terminal aneurysm) and at the basilar tip. The cerebral clipped aneurysms evaluated were IC–PC aneurysms, paracanoidal aneurysms, aneurysms at the anterior communication arteries (AcomAs), aneurysms at the middle cerebral arteries (MCAs), basilar tip aneurysms and aneurysms at the vertebral artery (VA). All of these were clipped using titanium clips.

Computed Tomography Scanning
At our hospital, CT was performed with 64 (GE Healthcare, LightSpeed VCT, Milwaukee, WI) or 32 detector rows (GE Healthcare, LightSpeed Pro 32), 120KV, Z-axis automatic tube current modulation (AutoM) (≤600mA), 0.625mm-section thickness, a field of view (FOV) of 25cm and a scanning time of 0.4 seconds per rotation. The scan range per rotation was 20mm (LightSpeed Pro 32) or 40mm (LightSpeed VCT). Non-ionic contrast medium (350 or 370mgI/ml) was injected using a power injector via a 20-gauge needle in the antecubital vein using a test-injection technique or an automatic trigger system. As a test injection, 10ml of contrast medium was injected at a rate of 4ml/second. A reference slice was used to monitor a region of interest in the cervical portion of the ICA to detect the arrival of contrast medium after injection. The proper delay was determined and the right or left common carotid artery was used as the reference point for the automatic trigger system. Acquisition of images started following the appropriate delay after injection of contrast medium. A total of 50ml
of contrast medium was administered at a rate of 4ml/second. Axial CT data were transferred to a 3D imaging workstation (Advantage Workstation, GE Healthcare).

**Image Processing and Results**

**Aneurysm Imaged Before Surgery**

A maximum intensity projection (MIP) image was first automatically obtained using the application for bone elimination (AutoBone Xpress, GE Healthcare Technologies) without any manual post-processing, taking approximately 20 seconds to obtain the first MIP images. The theory of bone elimination using this application has been reported previously. Volume-rendered (VR) images were obtained after the MIP images had been acquired (see Figures 1 and 2), and when almost no residual bone was visible, no further processing was necessary; however, approximately 80% of the patients required additional processing. Small bone remnants, which did not interfere with the image of the ICA or basilar artery, were visible near the ICA or basilar artery in approximately 50% of the patients and were easily removed from the image. Large bone remnants of the sphenoid and/or petrous bones were seen in approximately 10% of the patients; these were also able to be removed in this study (see Figure 3). Removal of part of the ICA siphon was most often seen due to dense calcification of the siphon of the ICA. When there was any dense calcification of an arterial wall in locations other than the siphon of the ICA, part of the relevant artery was also automatically removed by the application. However, further post-processing was able to recover all loss of the ICA image (see Figure 4). In a few cases part of the siphon of the ICA without calcification was removed by the application, although the mechanism is unclear. In cases with giant aneurysms with a wide neck, part of the parent arteries were removed because the giant aneurysms were not filled with contrast medium. In such cases, the parent arteries could be imaged after post-processing (see Figure 5). In our study, there was a significant difference in the visualisation of aneurysms and their necks between VR images processed with and without the application for bone elimination.11

**Clipped Aneurysms**

This application automatically removed the titanium clip images from the majority of aneurysms clipped with a single clip imaged using 3D
CTA (see Figure 6). Some post-processing was usually necessary to remove any remaining bones at the cranial base. Conventional 3D CTA sometimes overlooks remnant necks that are obscured by clips, and, if necessary, we were able to quickly and easily recreate the clips. In our study, when neck remnants of clipped aneurysms were present, 3D CTA with clip elimination was able to clearly visualise the neck remnants (see Figure 7). However, in aneurysms involving triple or quadruple clips, the metal artefacts obscured the presence or absence of the neck remnants.

**Discussion**

To date, a digital subtraction technique has usually been used to eliminate bones from CT images. This subtraction technique requires accurate registration during the entire acquisition, before and after contrast administration. In this case, a stereotactic frame to prevent movement of the head is used during data acquisition; however, this is uncomfortable for the patient. Moreover, the subtraction technique has the major disadvantage of requiring two scans, thus increasing the exposure of the patient to radiation. By contrast, the current method uses an image-processing application to eliminate bone structures at the base of the skull, instead of a subtraction technique. The current technique requires only one scan and therefore exposes the patient to a lower dose of radiation. Another advantage is a reduction of the time required to manually remove bony structures from images. The initial MIP images were automatically obtained within approximately 20 seconds. In the majority of cases, the remnant bones were small, only a few were near the ICA or basilar artery and most did not interfere with the ICA or basilar artery images. Remnant bones were easily removed from images through post-processing. Moreover, in the few cases in which large bone remnants were seen, these were easily removed through post-processing.

This technique has the major disadvantage of partial loss of vessel images on the initial MIP image. However, all images exhibiting a loss of vessels can be fully recovered through further post-processing. During post-processing, care must be taken in terms of the existence of small aneurysms at the site of the recovered artery and the site of remnant bone removal. This technique of employing an image-processing application for bone elimination is much more feasible for imaging aneurysms compared with conventional 3D CTA with bony structures. However, information regarding bony structures is critical for neurosurgeons prior to surgery; therefore, bone-free and conventional 3D CTA are complementary tools for imaging cerebral aneurysms before surgery. The current application for elimination of bones can also eliminate clips in cases of clipped cerebral aneurysms. Recognition of a residual aneurysm neck on post-operative angiography is of paramount importance, because incomplete treatment of an aneurysm may result in recurrent haemorrhage with serious or fatal consequences. There have been cases of small neck remnants re-growing over a long period into a dangerous aneurysm. IADSA has usually been used to evaluate clip placement in patients with clipped cerebral aneurysms; however, there have been a few previous reports suggesting the feasibility of 3D CTA after clipping surgery for cerebral aneurysms. These studies evaluated the use of
conventional 3D CTA with clips to replace IADSA, but 3D CTA with clip elimination could be significantly superior to conventional 3D CTA. 3D CTA using MDCT has the potential to replace IADSA to confirm complete or incomplete clipping of cerebral aneurysms in cases involving no more than one or two clips. MR angiography (MRA) also provides 2D and 3D images of aneurysms without bony structures. There are several limitations in imaging aneurysms by MRA. Flow-related artefacts can result in under-estimation of the size of aneurysms. Even in larger aneurysms, turbulent flow and/or thrombosis within the aneurysm can cause poor visualisation of the aneurysm by MRA. However, MRA using 3 Tesla (3T) MR systems is able to clearly image small aneurysms. Further studies should compare the current bone-free CTA technique with MRA. Moreover, to determine whether bone-free 3D CTA is a viable alternative to IADSA, detection of aneurysms should also be compared between 3D CTA and IADSA in a blinded study.

**Conclusion**

Bone-free 3D CTA using an image-processing application for the elimination of bones can improve delineation of cerebral aneurysms near the skull base. This technique does not increase radiation exposure to patients, and remnant bones in the initial MIP images automatically acquired by the application for bone elimination can be easily removed through post-processing. Although parts of vessels are sometimes removed from the image along with the bones, these can be quickly and easily recovered through post-processing. Thus, bone-free 3D CTA and conventional 3D CTA are complementary tools for imaging cerebral aneurysms near the skull base prior to surgery. This application can also eliminate clips in cases of clipped cerebral aneurysms. 3D CTA with the elimination of clips can improve the accuracy of detecting remnant necks after clipping surgery, and may be a viable alternative to IADSA for the detection of remnant necks in cases with single or double clips.

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